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Massachusetts  
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Technology

# Nature-Inspired Biomimetic MEMS/NEMS Sensors for wireless Sensing

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MIT Sea Grant College Program

Massachusetts Institute of Technology (MIT)

# Background



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Massachusetts  
 Institute of  
 Technology



Singapore-MIT Alliance for Research and Technology

Assistant Professor at RUG  
 Principal Research Scientist  
 Postdoctoral Associate  
 Associate Scientist at MIT

2018 - present  
 2015- 2017  
 2014-2015  
 2013-present

PhD 2010-2013



NANYANG  
 TECHNOLOGICAL  
 UNIVERSITY

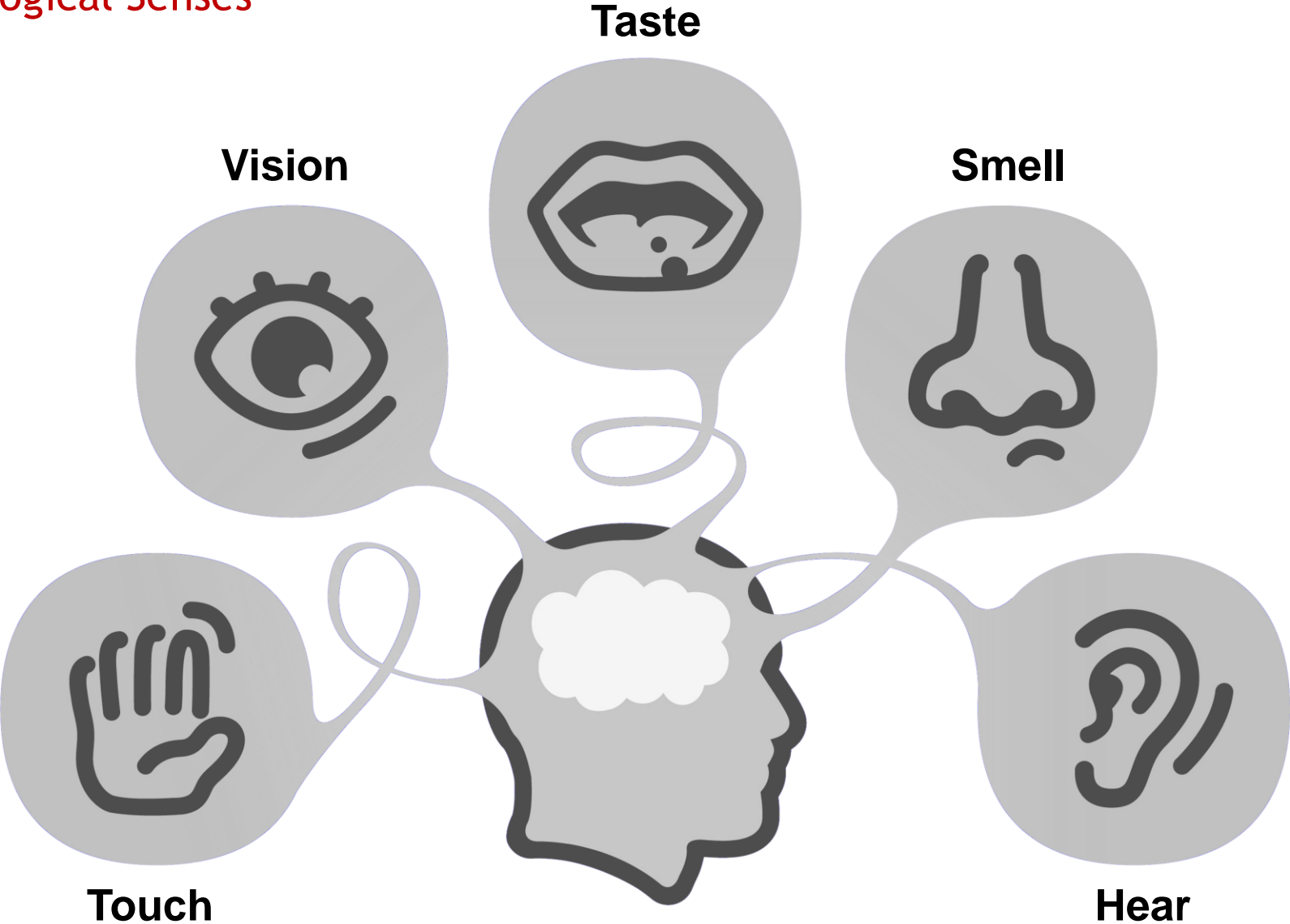
Singapore-MIT Alliance Graduate Fellowship  
 Nanyang Technological University (NTU) and  
 Massachusetts Institute of Technology (MIT)



Massachusetts  
 Institute of  
 Technology

Masters in Technology (M.Tech) Solid State Technology 2007-2009  
 Masters in Physics (M.Sc) with Hons. (Photonics, Specialization) 2005-2007  
 B.Sc (Physics) with Hons. 2002-2005

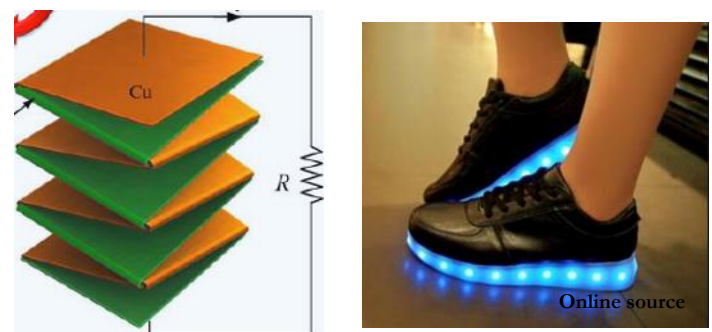
# Biological Senses



# Biomimetic Micro/Nano Electromechanical Systems (MEMS/NEMS)



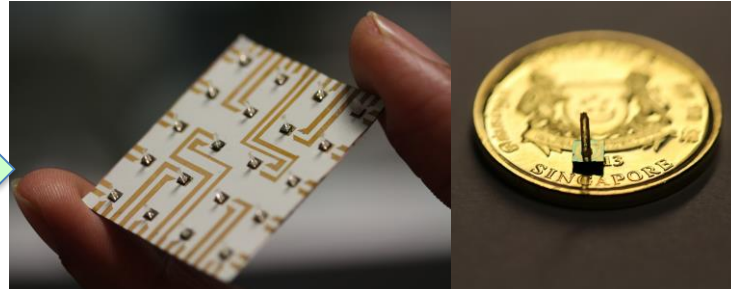
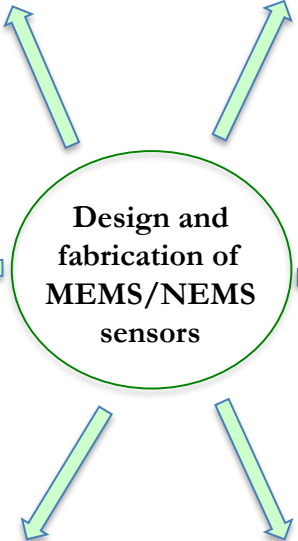
Biomimetic MEMS flow Sensors inspired by the superficial neuromasts in blind cavefish



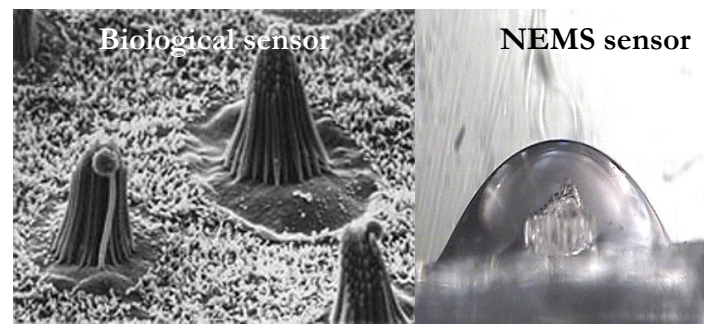
Origami-inspired energy harvesters for wearables



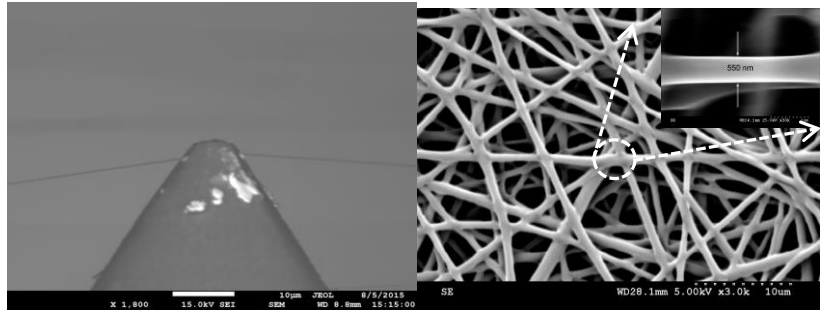
Harbor seal whisker inspired MEMS flow sensors to reduce vortex-induced vibrations



Artificial smart skin of flexible and self-powered MEMS flow sensors



Ultrasensitive artificial NEMS ciliary bundles inspired by mechanotransduction in biological sensors in nature



Electronic sensing materials for flexible, 4 wearable and stitchable sensors

# **Neuromast Inspired Flow Sensors for Fish-Like Underwater Sensing**

# Background: Bioinspiration – Blind cavefish



*Astyanax mexicanus fasciatus*



*\*Hydrodynamic imaging: Blind cave fish in a tank with lego obstacles*



Source: Video from Lauder G V, Harvard

*Energy efficient maneuvering: Fish performing Karman gaiting behind a D-shaped cylinder*

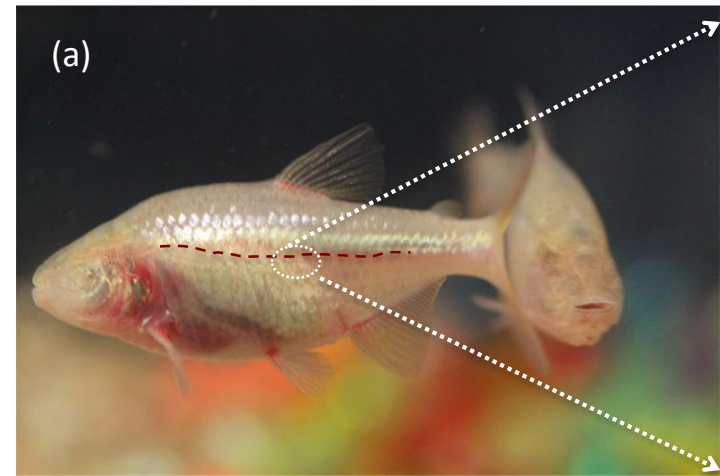


Source: Video from Lauder G V, Harvard

*Control and maneuvering: Fish escape response through flow Sensing*

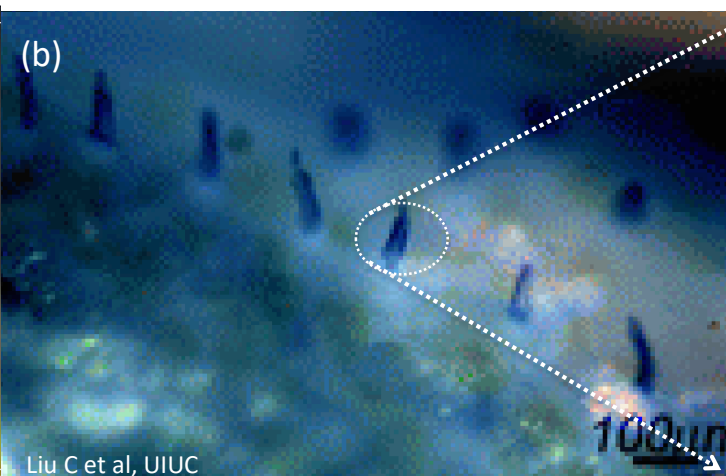
# Superficial neuromast (SN) sensors

## Superficial neuromasts and flow sensing



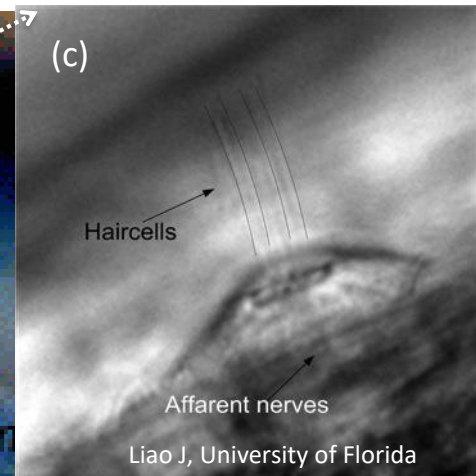
(a)

(a) Bio-inspiration: Blind cave fish



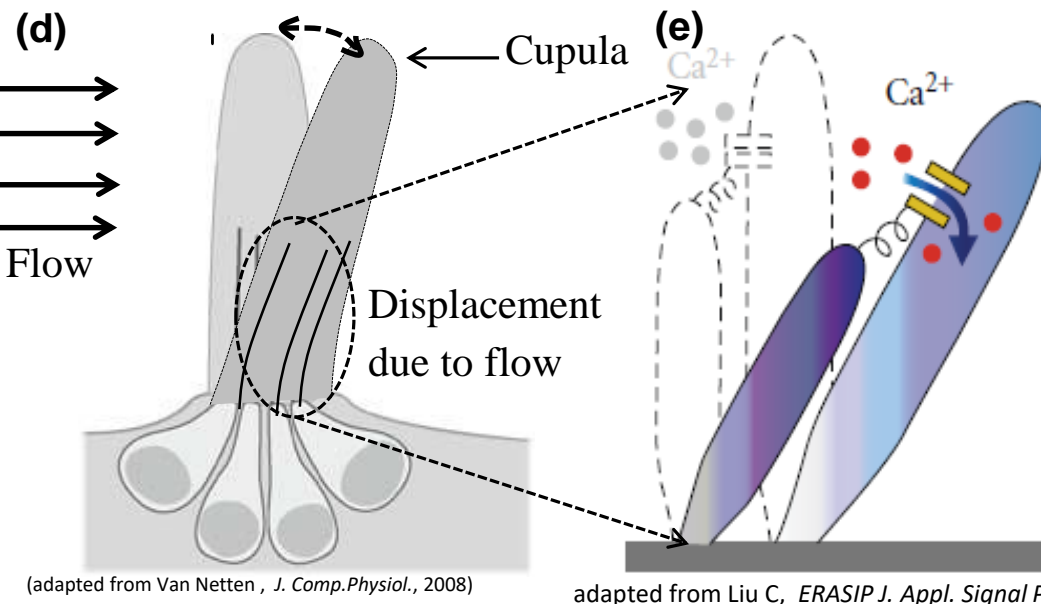
(b)

(b) SEM image of the lateral-line



(c)

(c) Single biological neuromast



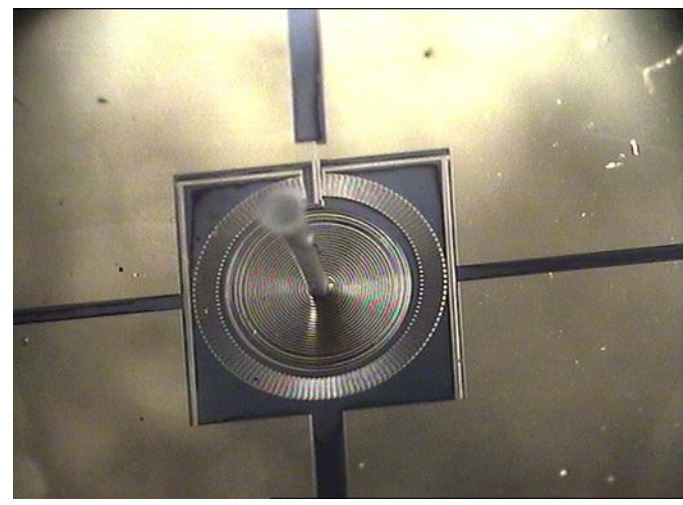
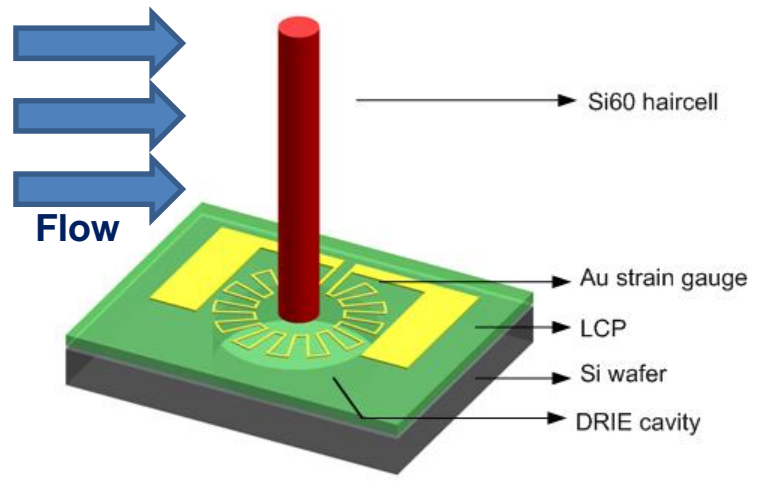
(adapted from Van Netten, *J. Comp. Physiol.*, 2008)

adapted from Liu C, *ERASIP J. Appl. Signal Process.*

(d) and (e) Sensing principle

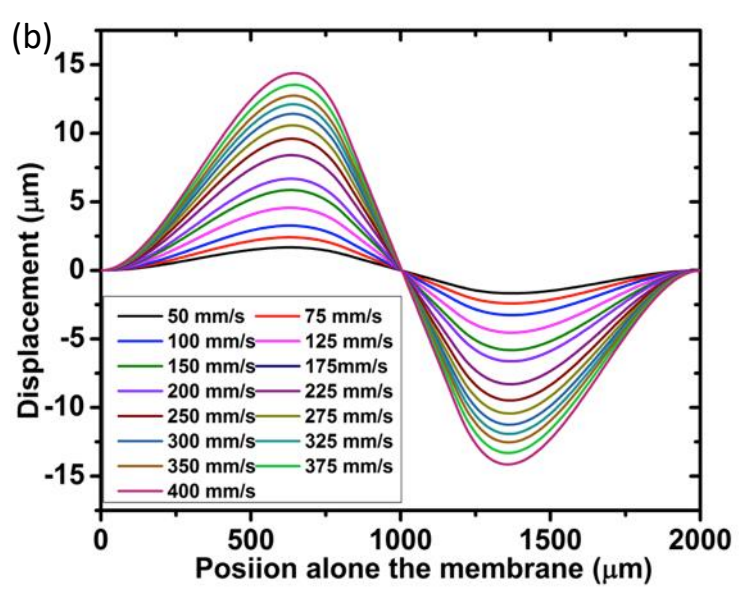
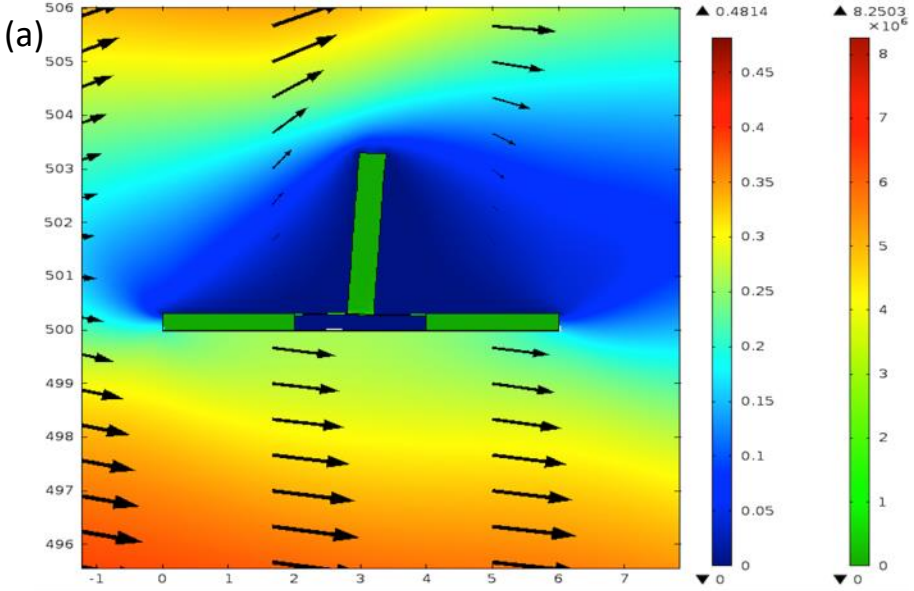
- Located on the surface of the skin
- Cupula couples flow to the embedded haircells & increases drag force
- Tiny haircells- key sensing elements
- Measure relative flow between the body and the surroundings.
- Hydrodynamic flow mapping on the entire body

# LCP haircell sensor design



Structure of LCP MEMS Haircell sensor

SU-8 haircell on LCP membrane



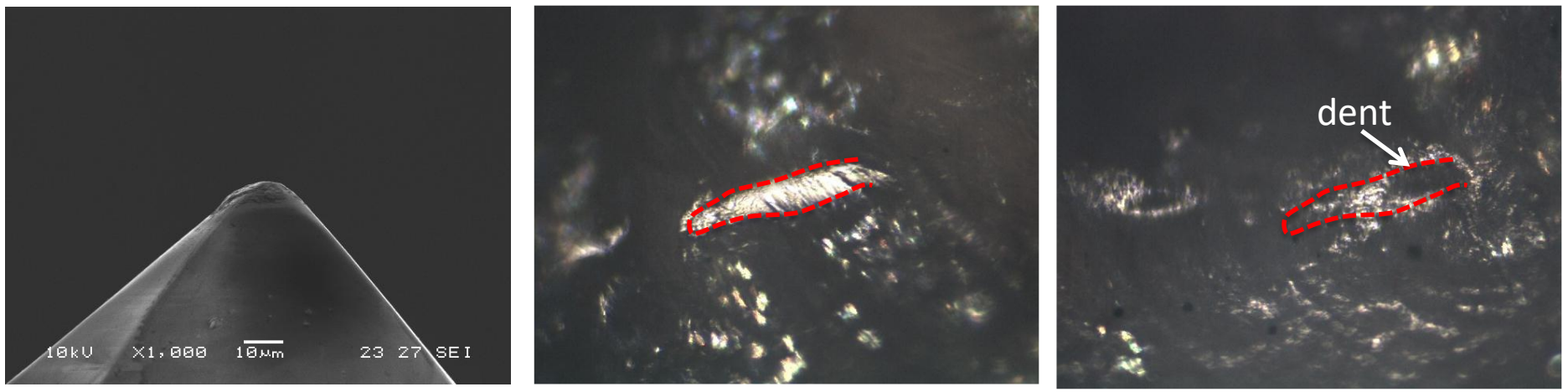
COMSOL finite element simulation results (a) membrane displacement in response to a water flow velocity of 0.5m/s (b) displacement profile of the membrane for various water flow velocities

The high-aspect ratio haircells reach beyond the flow generated by the boundary layers and results in enhanced sensitivity

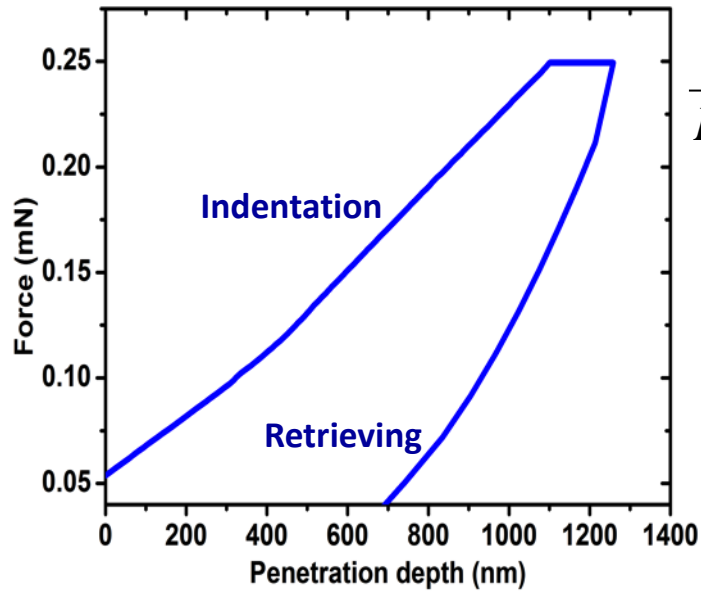


# Biomimetic materials for cupula

## Biological cupula



SEM and optical images of (a) Cono-spherical tip used for indentation. Cupula surface (b) before and (c) after indentation



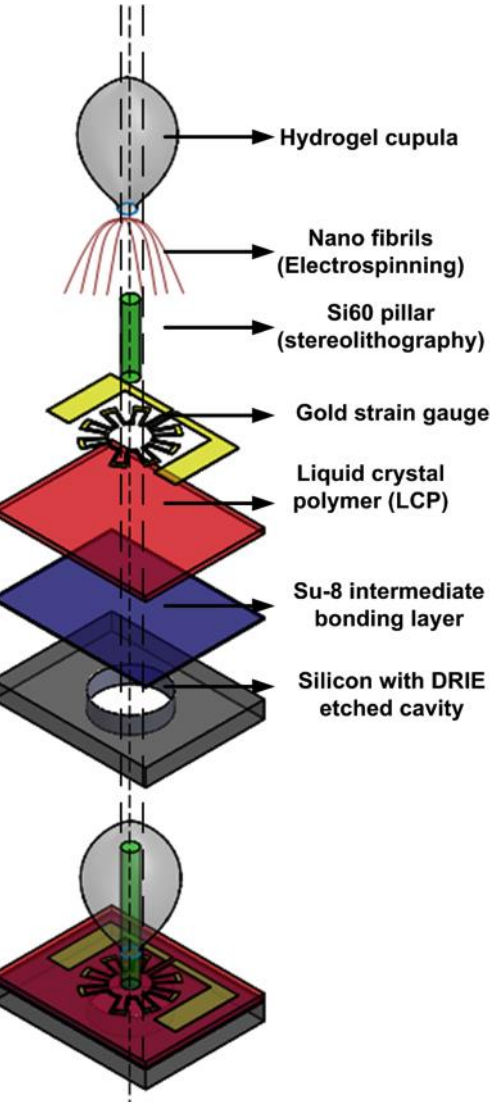
$$\frac{1}{E_r} = \frac{1-\nu_i^2}{E_i} + \frac{1-\nu_s^2}{E_s}$$

subscript *i* and *s* refer to indenter and sample materials, and  $\nu$  refers to Poisson's ratio,  $E_r$  reduced modulus (the combined modulus of the tip and the sample)

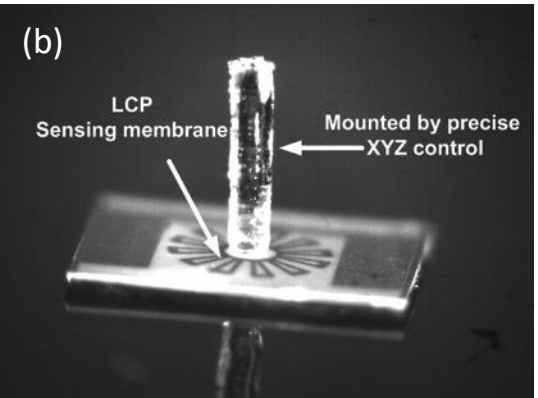
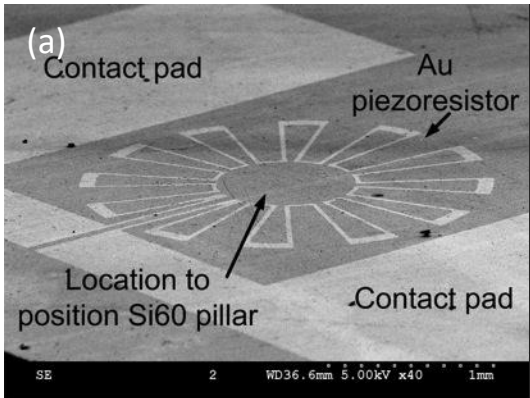
- Hardness = 40kPa
- Young's modulus ( $E$ ) = 138kPa
- Observed  $E$  is much higher than the values reported in the past
- Sample preparation methods resulted in higher  $E$  value

# Biomimetic Artificial Neuromast Sensor

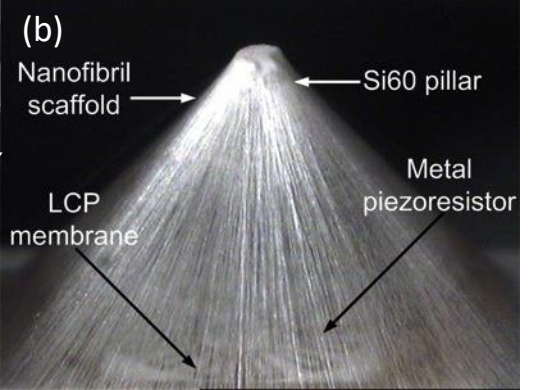
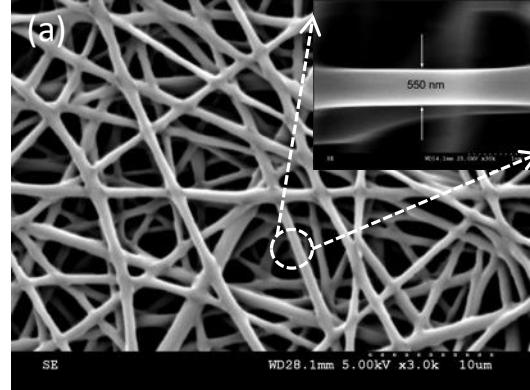
## Sensor fabrication



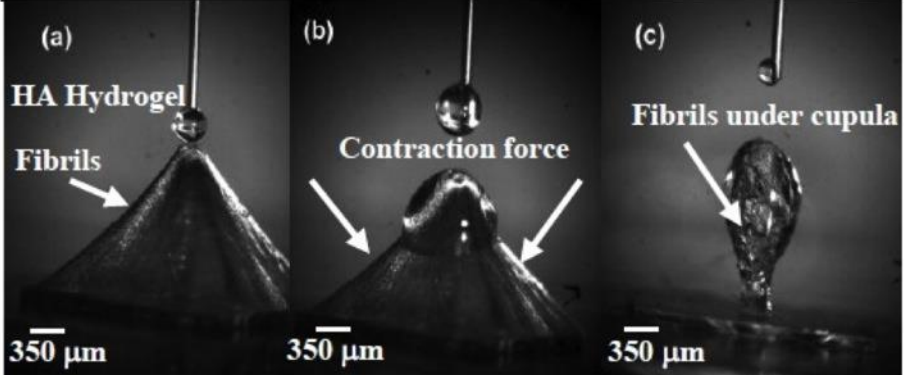
A schematic showing the exploded view of the fabrication scheme designed to form MEMS artificial neuromast sensor



(a) LCP sensing membrane (b) Naked haircell sensor



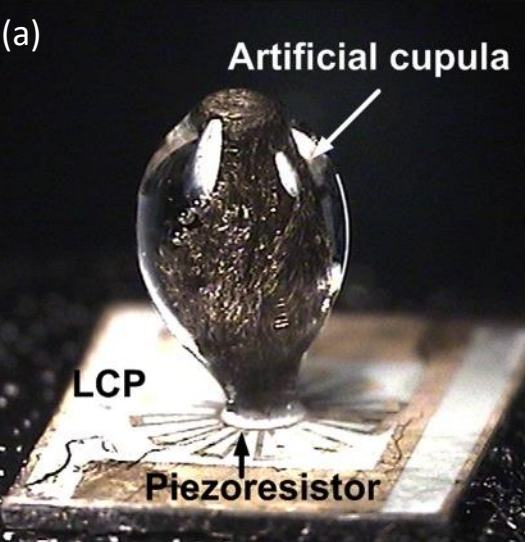
Electrospinning to form cupular fibrils (a) nanofiber optimization (b) Electrospun scaffold



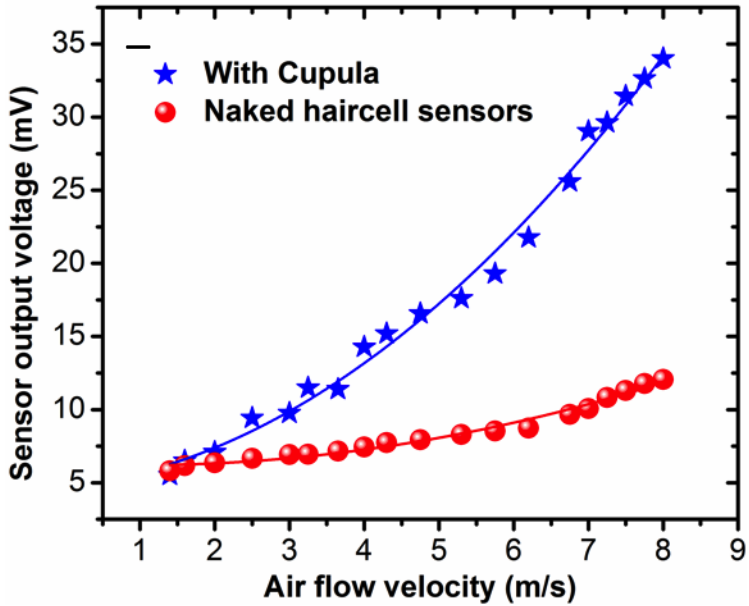
HA-MA Hydrogel drop-casting process

# Flow sensing abilities of the MEMS neuromast

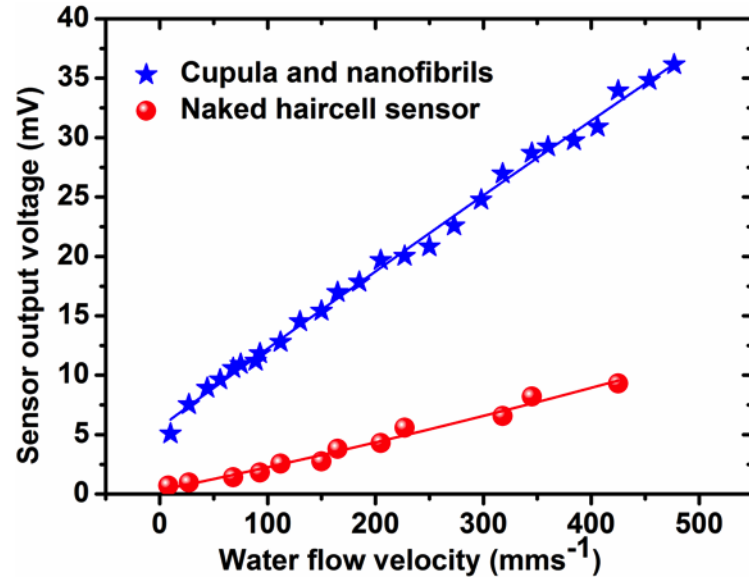
## Experimental Results



Microscopic images of (a) MEMS Artificial neuromast flow sensor  
(b) Zoom-in view showing the encapsulated cupular fibrils



Wind tunnel flow calibration results



Water tunnel flow calibration results

## Achievements

- Ultrahigh sensitivity
  - 4.5mV/(m/s) for air flow
  - 5 times enhancement
  - 0.08mV/(mm/s) for water flow
  - 3.5 times enhancement
- Threshold detection limits
  - 0.01m/s for air flow
  - 20mm/s in water flow
- Enhanced accuracy
  - VIV reduction
  - Reduced turbulence
- Robustness
  - Reliable materials
  - 20m/s air flow
  - 3m/s water flow

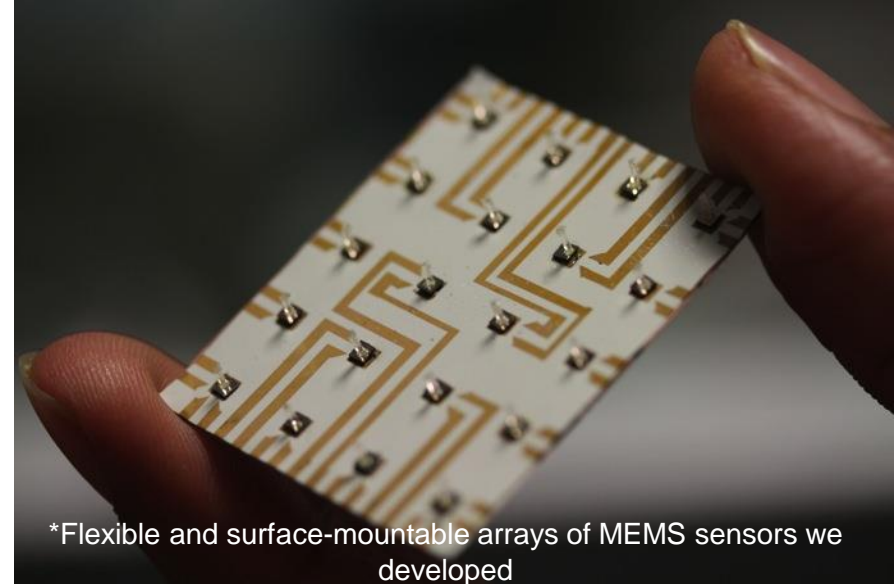
$$\left(\frac{F_{cupula}}{F_{hair}}\right) \approx \left(\frac{H_{cupula}}{H_{hair}}\right)^{4/3} \left(\frac{D_{cupula}}{D_{hair}}\right)^{2/3}$$

- F – drag force
- H – height
- D – diameter
- Subscript c – cupula and h – haircell

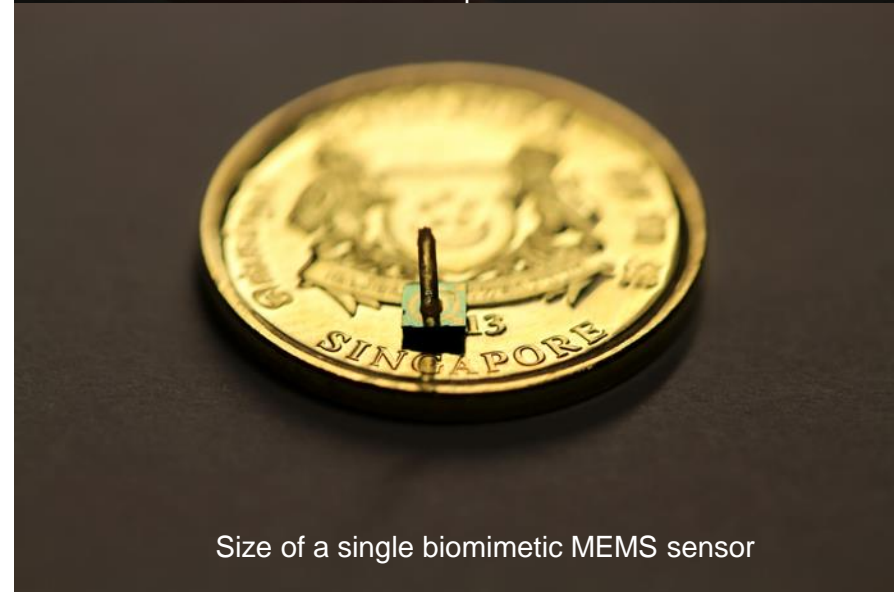
\*Ajay Kottapalli et al, Asia Materials (Nature Publication Group), 2017, 9, e440

# Zero-Powered Flow Sensors

- Fundamentally, it is possible to translate complex mechanosensory sensing principles found in nature onto an artificial sensory platform using MEMS technology
- MEMS/NEMS sensors can be fabricated with various structural configurations and materials and at the dimensions of biological sensors
- Features of our MEMS flow pressure sensors
  - Ultrahigh sensitivity
  - Extremely low threshold detection limits
  - Self-powered
  - Miniaturized
  - Robust and reliable
  - Low cost
  - Packaged in to flexible surface-mountable arrays
  - Biomimetic signal amplification and noise rejection strategy



\*Flexible and surface-mountable arrays of MEMS sensors we developed

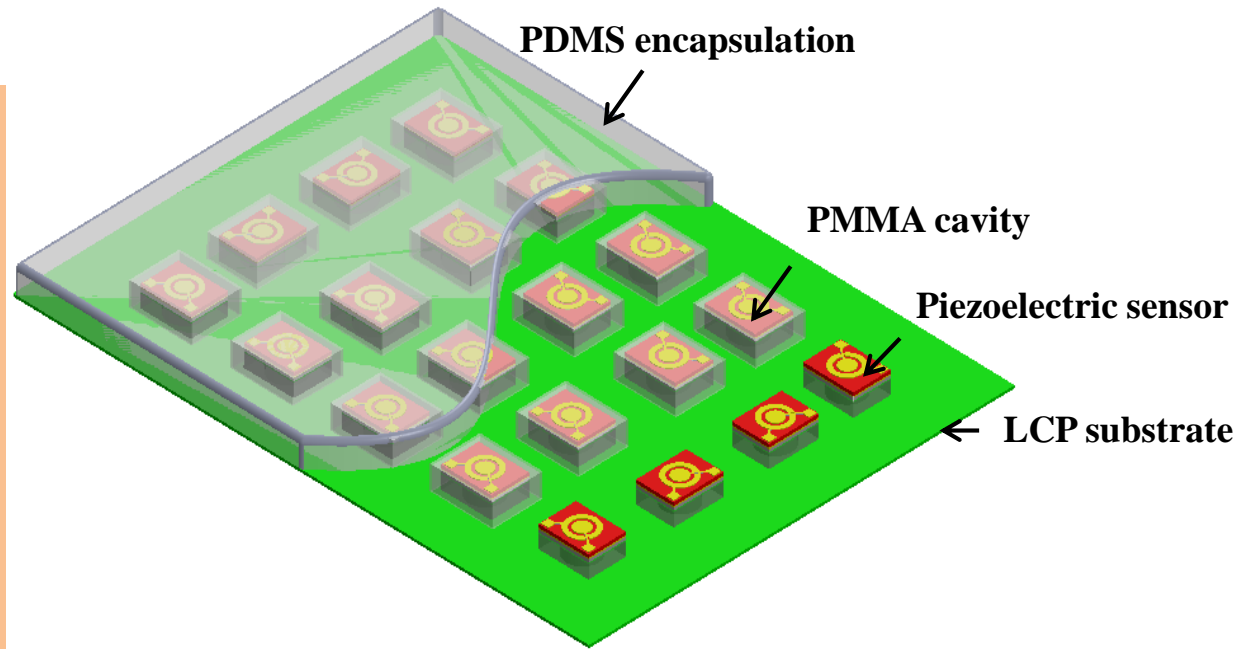


Size of a single biomimetic MEMS sensor

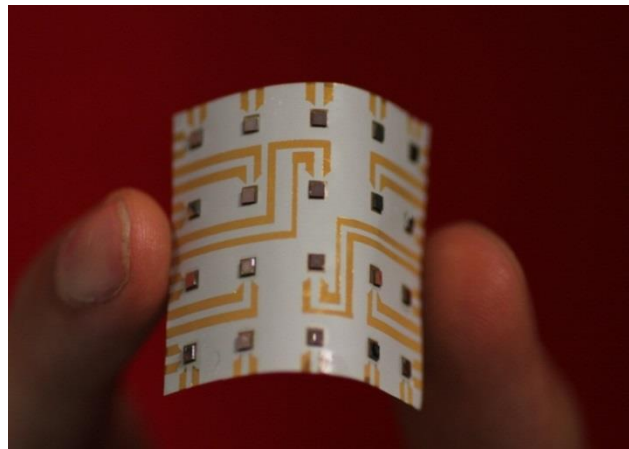
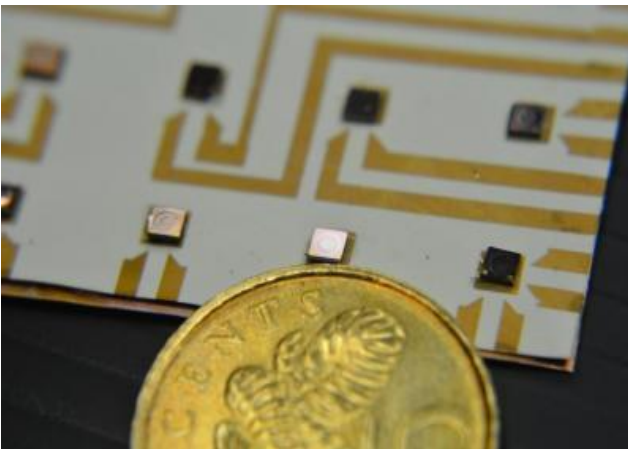
# Packaging

## Key points:

- Flexibility
- Surface mountable
- Under water protection
- Stability in harsh environment

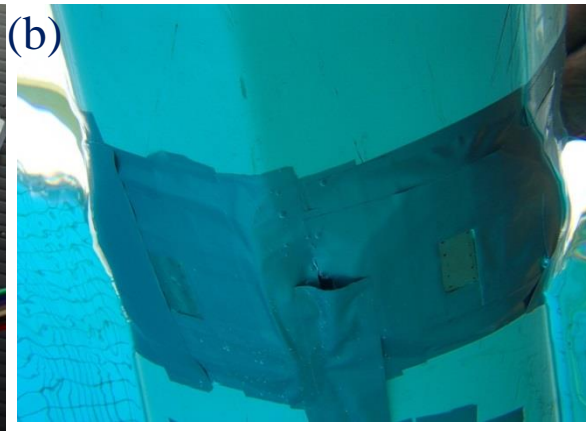
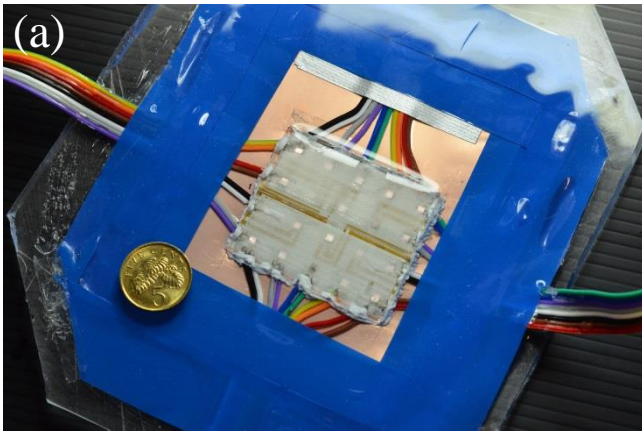


Schematic view of the array of  $4 \times 5$  sensors

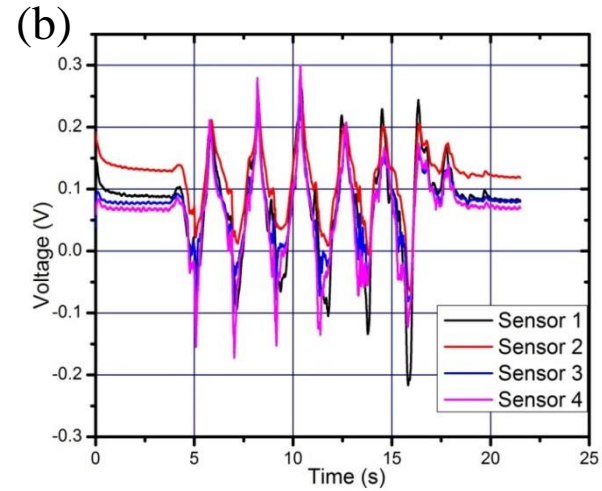
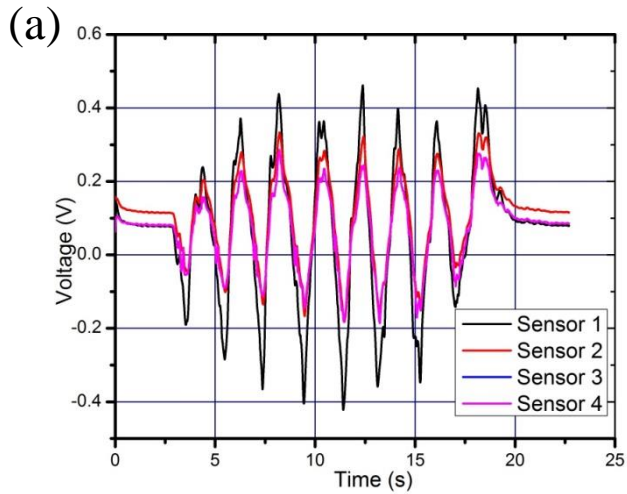


Array of  $4 \times 5$  of the piezoelectric sensors mounted on flexible LCP

# Real-time underwater sensing

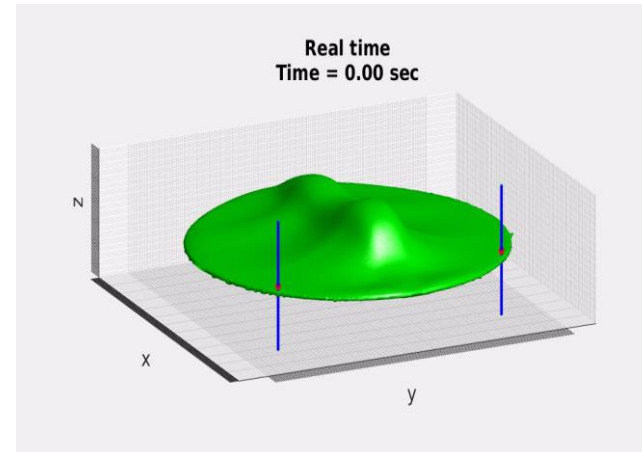
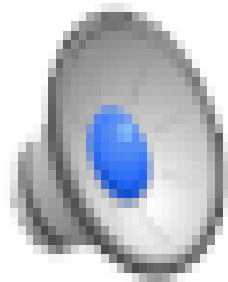


(a) Array of 4 by 5 of proposed (b) The sensors were surface mounted on the kayak and submerged in water for experiment



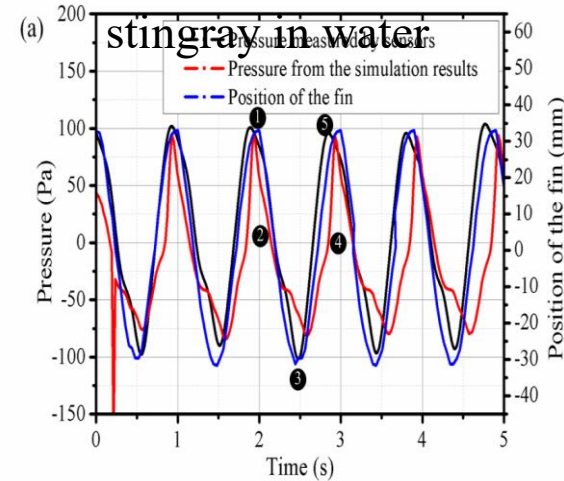
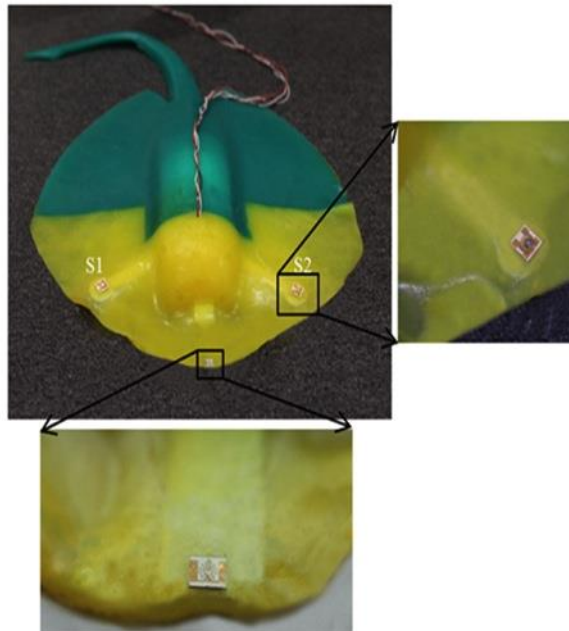
(a) A signal generated by manually lifting and pushing the kayak up and down in water (b) A signal generated by rolling the kayak side to side in the water

# Sensing Real-Time Hydrodynamics on a Robotic Stingray

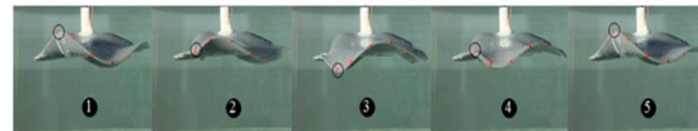


3-dimensional simulation of the robotic

stingray



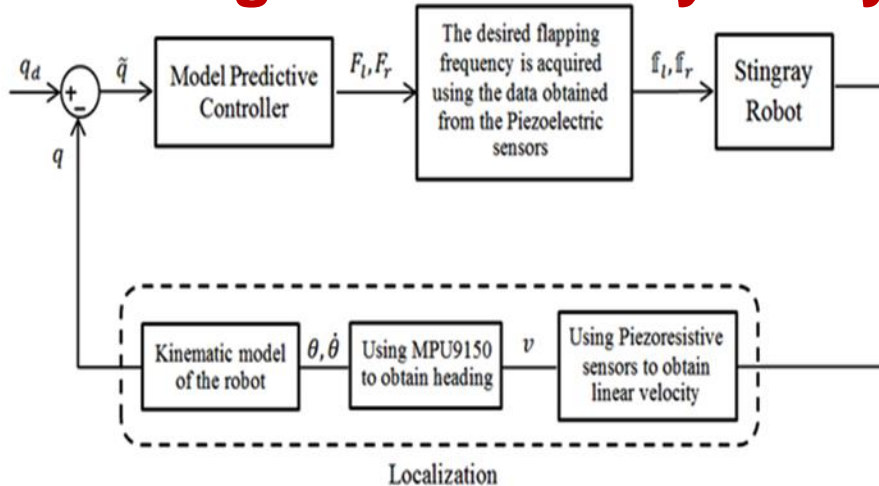
(b)



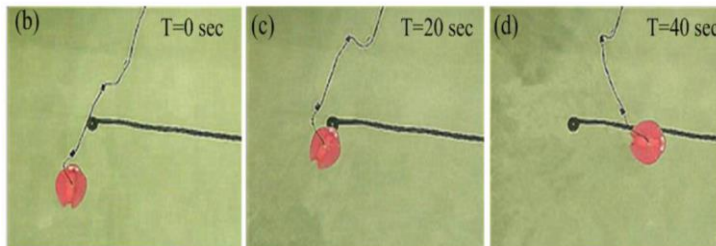
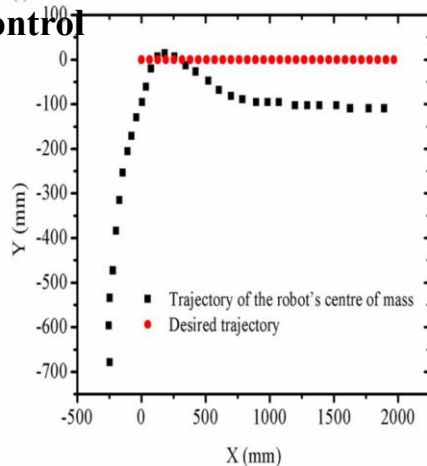
Sequence of images taken as the

MEMS pressure and flow sensors mounted on stingray flaps at a frequency of 1Hz  
the robotic stingray (Courtesy: Pablo v Alvarado)

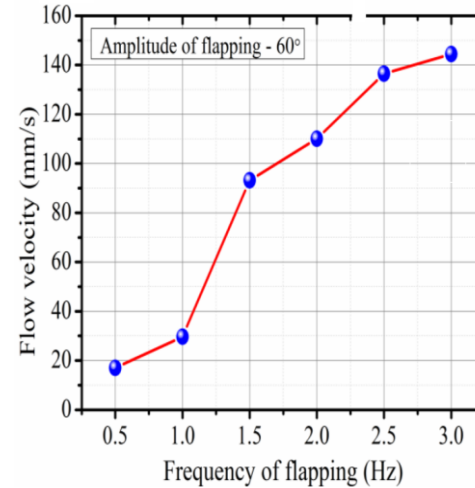
# Sensing Real-Time Hydrodynamics



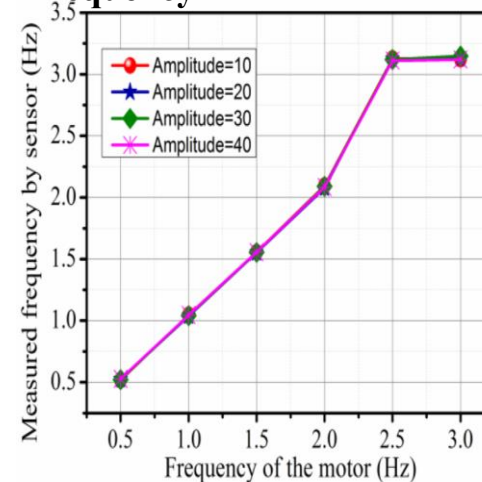
The block diagram of the proposed feedback control



(a) Trajectory of the robot's center (b) Snapshot of the robot at different time instances



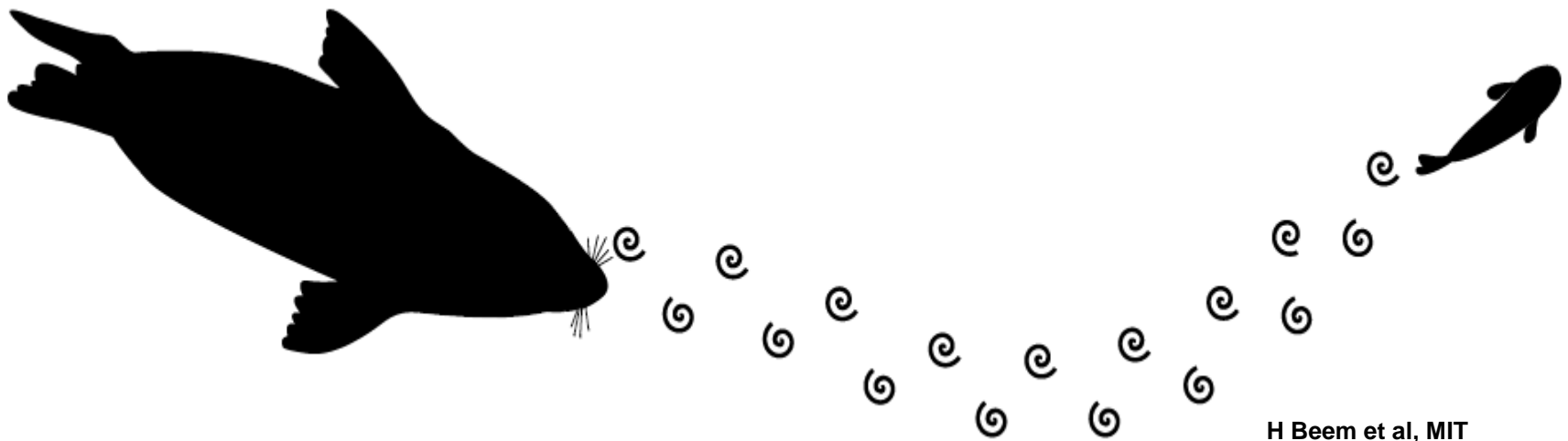
velocity of propagation of the robot with respect to fin flapping frequency



Comparing the measured frequency and the actual frequency of the fin



# Seal Whisker Inspired Flow Sensors



H Beem et al, MIT

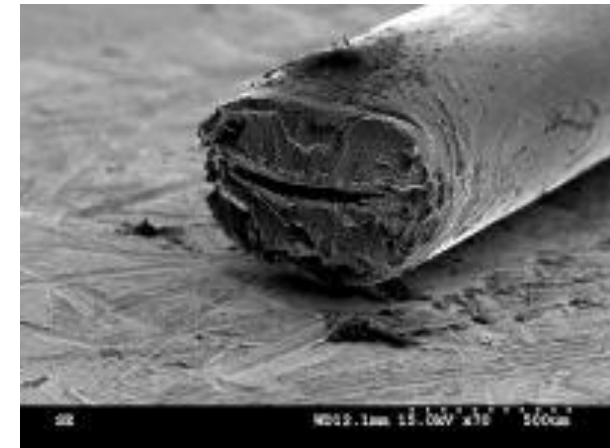
# Seal-whisker and flow sensing



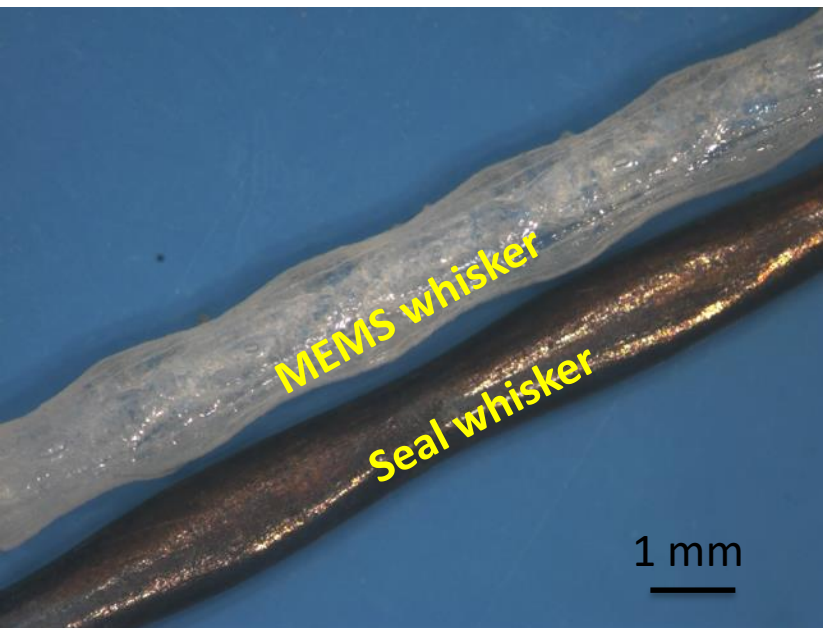
Harbor Seal (*Phoca Vitulina*)



Microscopic image showing the Undulatory whisker geometry



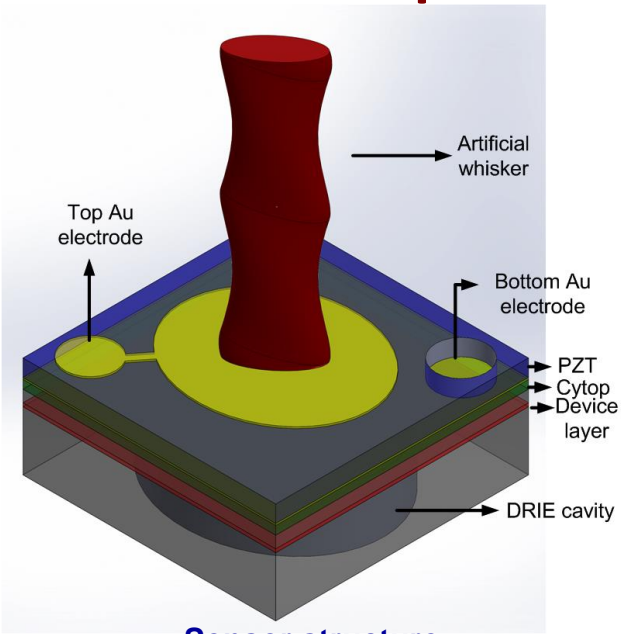
Cross-section of the whisker reveals no muscle



Artificial micro-whisker with undulatory geometry

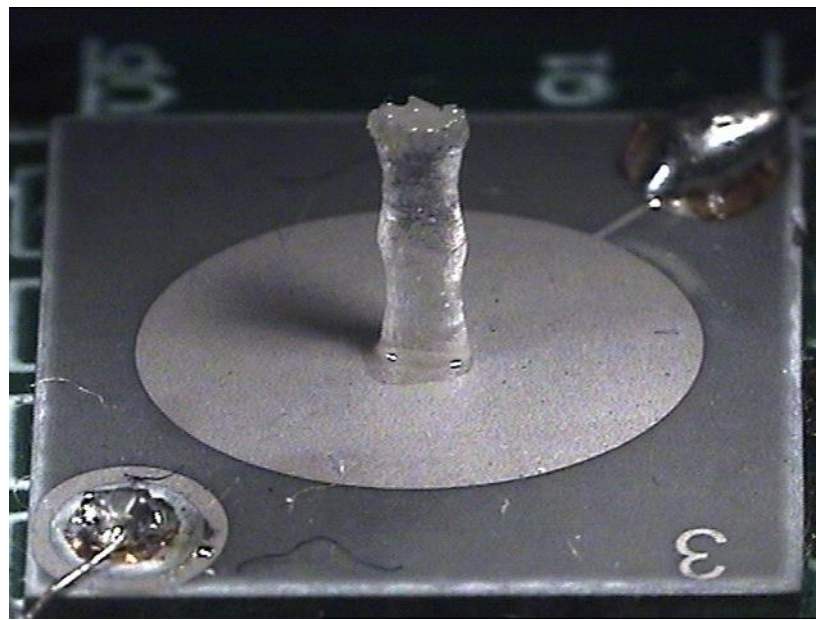
- Complex 3D geometry with elliptical cross-section
- Undulations on major and minor axis
- Capable of detecting the wake of a fish up to 35s after the fish has passed.
- Unique undulatory geometry is believed to have a contribution towards reducing vortex-induced vibrations experienced
- Achieve ultrahigh sensitivity  $245 \mu\text{m/s}$

# Seal-whisker inspired MEMS flow sensor

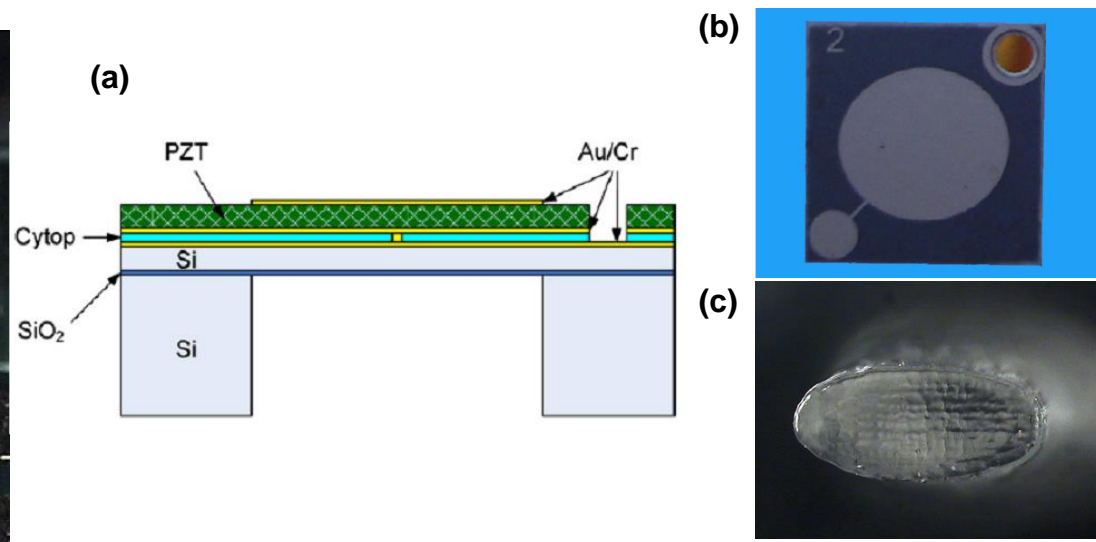


Sensor structure

- Piezoelectric sensing membrane
- Micro-whisker fabricated by stereolithography
- Micro-whisker structure interacts with flow.
- Flow variations cause displacement of the whisker which in turn causes the PZT membrane to bend
- Charges generated by membrane bending are calibrated to flow velocity that the whisker faces

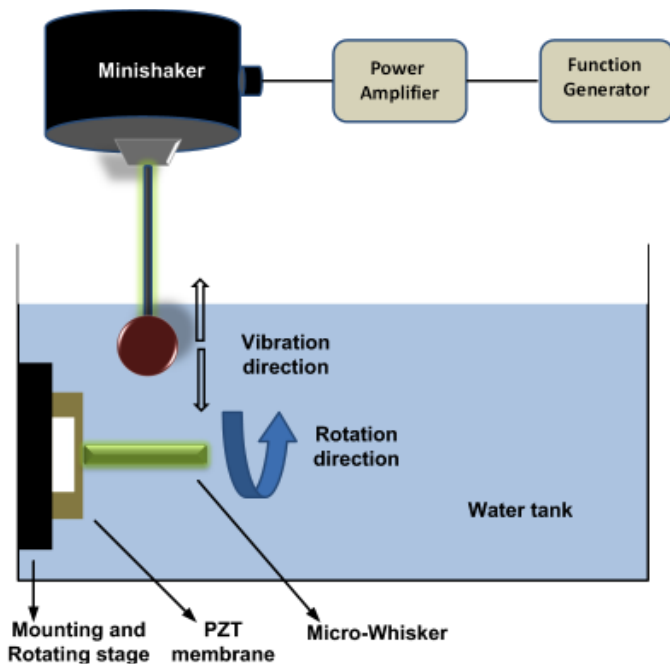


Optical microscopic image of the sensor

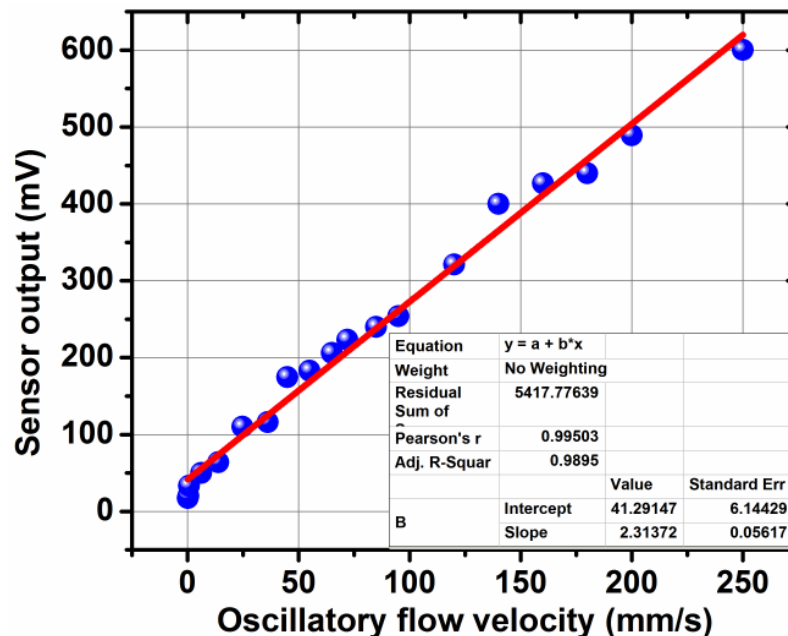


Sensor fabrication process (a) Various sensing layers in the membrane (b) Top-view of the PZT membrane (c) Flat mountable base of the whisker

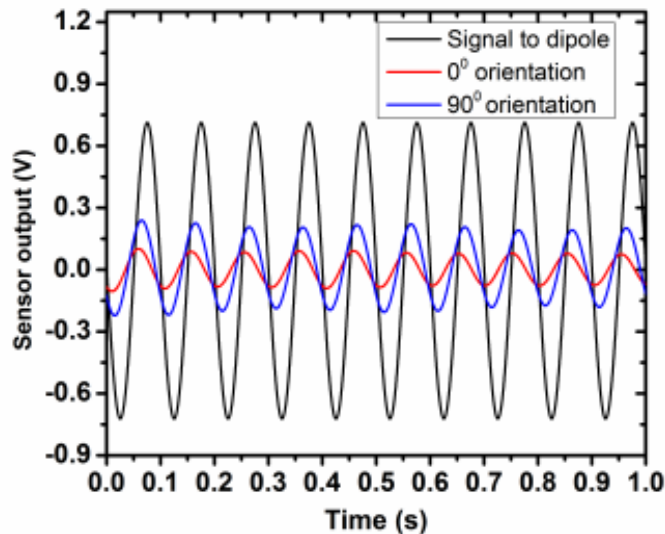
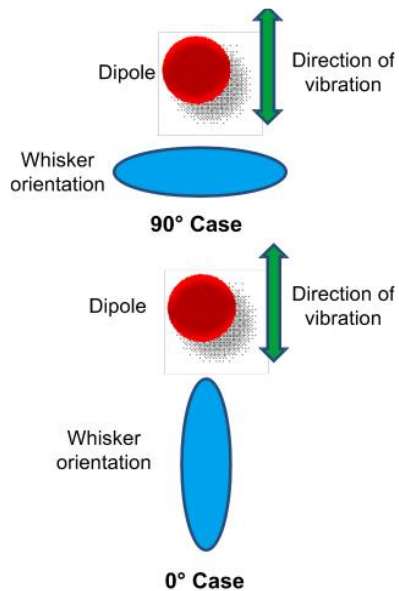
# Whisker inspired sensor flow characterization



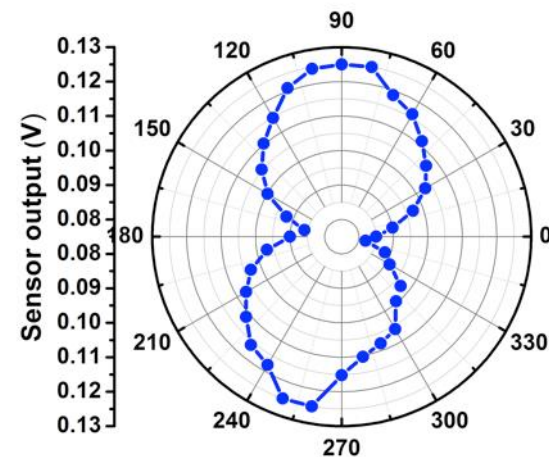
Schematic of the experimental set-up



Oscillatory water flow velocity sensing



Directional dependence of the MEMS whisker sensor output due to its elliptical cross-section



# **Journey from lab-to-market**

# Market Size & Adjacencies: Lucrative Options Abound



Respiratory  
Care



Hospital  
Infusion  
Pumps



Misc. Medical  
- Urine Flow



SENSORNOMICS



Industrial  
Applications

Ambulatory  
Pumps



# Infusion Pump: A Blessing With Flaws (Sometimes Fatal)



**What If We Can Read The Live Infusion Rates?**

**A New Standard of Care?**



# Funding, Team and Roadmap

2014



**Innovation Centre**

inspired by the Deshpande Center at MIT

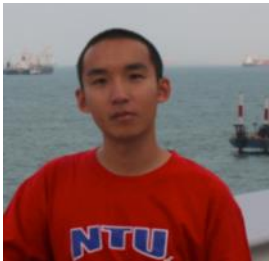
Fund of 450,000 S\$

≈ 300,000 Euros

Biomimetic microsensors for flow monitoring in Intravenous infusions, urine drainage and sleep apnea applications



2014-16



Dr. Shen Zhiyuan  
(Postdoc)



Mr Vignesh  
(Research Engineer)



Dr Mohsen  
(Post Doc)



Mr Irwin  
(Business consultant)

Team formation  
Supervision



2016



**SENSORNOMICS**

Start-up

Creating New Standards of Care with the Future of Flow Sensing

Thank you for your patient listening.....

